

RESEARCH ARTICLE

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Preliminary evaluation of prototype footwear and insoles to optimise balance and gait in older people

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Abstract

Background: Footwear has the potential to influence balance in either a detrimental or beneficial manner, and is therefore an important consideration in relation to falls prevention. The objective of this study was to evaluate balance ability and gait patterns in older women while wearing prototype footwear and insoles designed to improve balance.

Methods: Older women ($n = 30$) aged 65 – 83 years (mean 74.4, SD 5.6) performed a series of laboratory tests of balance ability (postural sway on a foam rubber mat, limits of stability and tandem walking, measured with the Neurocom® Balance Master) and gait patterns (walking speed, cadence, step length and step width at preferred speed, measured with the GAITRite® walkway) while wearing (i) flexible footwear (Dunlop Volley™), (ii) their own footwear, and (iii) prototype footwear and insoles designed to improve dynamic balance. Perceptions of the footwear were also documented using a structured questionnaire.

Results: There was no difference in postural sway, limits of stability or gait patterns between the footwear conditions. However, when performing the tandem walking test, there was a significant reduction in step width and end sway when wearing the prototype footwear compared to both the flexible footwear and participants' own footwear. Participants perceived their own footwear to be more attractive, comfortable, well-fitted and easier to put on and off compared to the prototype footwear. Despite this, most participants ($n = 18$, 60%) reported that they would consider wearing the prototype footwear to reduce their risk of falling.

Conclusion: The prototype footwear and insoles used in this study improve balance when performing a tandem walk test, as evidenced by a narrower step width and decreased sway at completion of the task. However, further development of the design is required to make the footwear acceptable to older women from the perspective of aesthetics and comfort.

Trial registration: Australian New Zealand Clinical Trials Registry. ACTRN12617001128381, 01/08/2017 (retrospectively registered).

Keywords: Ageing, Falls, Postural balance, Footwear

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Background

Falls in older people are a major public health problem [1]. By modifying the interface between the body and the environment during weightbearing activities, footwear has the potential to influence balance in either a detrimental or beneficial manner, and is therefore an important consideration in relation to falls prevention. Several laboratory-based studies have demonstrated that elevated heels [2–4] and thick, soft soles [3–5] are detrimental to balance, while footwear with high collars [3, 6–9] and firm soles [4, 7, 8] are beneficial. Prospective studies have also shown that wearing shoes with slippery soles [10], high heels [11, 12] and reduced sole contact area [12] increase the risk of falls in older people. This is of particular concern for older women, as many styles of female footwear incorporate these potentially hazardous features.

In response to these observations, it has been suggested that the ideal safe shoe for older people at risk of falling should have a low, broad heel, a thin, firm midsole, a high collar and a textured, slip-resistant outersole [13, 14]. However, although this recommendation is a valid summary of the available literature, very few commercially available footwear styles incorporate all of these features, particularly with regard to female footwear. Furthermore, in order for such a recommendation to be widely adopted, such footwear needs to be acceptable to older people from the perspective of comfort, ease of use and aesthetics [15]. Therefore, the objectives of this study were to (i) evaluate balance ability and gait patterns in older women while wearing prototype footwear and insoles designed to improve balance, and (ii) investigate older women's perceptions of the footwear.

Methods

Participants and assessments

This study was conducted alongside an investigation into the effects of indoor footwear on balance in community-dwelling older women [16]. These studies evaluated the same participants but laboratory testing was performed on two different occasions (one session for indoor footwear and one session for outdoor footwear). Full details of the methods, including participant eligibility, questionnaires, clinical, falls risk, balance and gait assessments and perceptions of footwear have been published [16]. Apart from the footwear conditions assessed, the only other methodological difference between the two studies was that balance testing in the current study was performed when standing on a foam rubber mat rather than on the floor. The balance testing protocol is shown in Fig. 1. Ethical approval was granted from the La Trobe University Faculty of Health Sciences Human Ethics Committee (Reference FHEC14/254), and written informed consent was obtained from all participants.

Footwear conditions

Participants performed each of the balance and gait assessments under three footwear conditions: (i) flexible footwear, (ii) their own footwear, and (iii) the prototype footwear and insoles. For the flexible and prototype footwear, appropriate sizing was determined using the Brannock device® [17]. The order of testing was randomised to avoid order effects.

The flexible footwear (Dunlop Volley™, Pacific Brands, Australia) had a rubber sole of uniform 18 mm thickness, a hardness of Shore A 35 [18], and lace fixation. Across the size range, the weight of the flexible footwear was 280 – 420 g. The flexible footwear was selected as a control condition as it had no features considered to be either beneficial or detrimental to balance and could therefore be considered a 'minimalist' style of shoe [19].

For the 'own footwear' condition, participants were asked to bring to the testing session the footwear they wore most often when outdoors. The characteristics of the footwear were assessed and documented using selected items from the Footwear Assessment Tool [20].

The prototype footwear was based on an existing model and was manufactured by Dr. Comfort® Footwear (Mequon, WI, USA). The base model (the 'Vigor') was selected as it incorporates many of the features previously shown to be beneficial for balance. Specifically, the footwear had a firm (Shore A hardness 55 [18]) rubber sole of 25 mm thickness under the heel and 18 mm under the forefoot, laces plus Velcro® fastening, a high collar to support the ankle, and a firm heel counter. Across the size range, the weight of the prototype footwear was 310 – 360 g. To create the prototype, the outersole was modified to optimise slip resistance by grinding a 10 degree bevel into the heel region [21, 22], placing grooves perpendicular to the sole (1.2 mm deep and 2.4 mm wide) across the heel surface area [23], and placing perpendicular grooves (5 mm deep and 12 mm wide) across the rest of the sole [24, 25]. A textured insole was also constructed from 4 mm thick ethyl vinyl acetate (Shore A 25 [18]) with dome-shaped projections (3 mm high and 8 mm diameter, Shore A 85 [18]) placed across the forefoot in a 15 mm diamond pattern and along the lateral border, extending to the heel. The design of the textured insole was informed by previous studies reporting improvements on balance in older people when similar insoles were worn [26, 27]. Figure 2 shows key features of the prototype footwear.

Statistical analysis

Statistical analysis was undertaken using SPSS Version 22.0 (IBM, Armonk, NY, USA). Participants who had missing data because they were unable to complete the task were given the 'worst' score of the remaining sample. Differences between the three footwear conditions

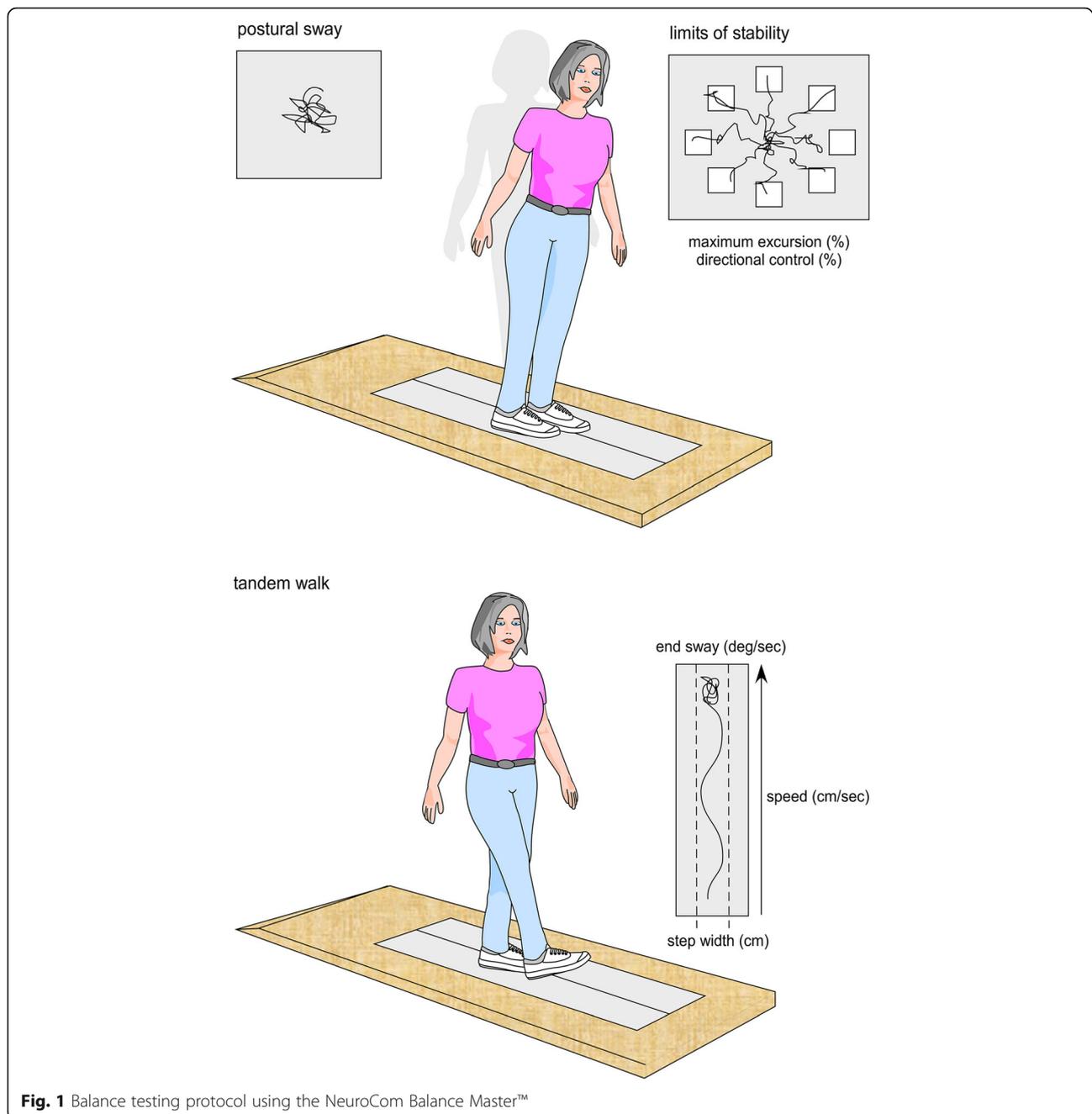


Fig. 1 Balance testing protocol using the NeuroCom Balance Master™

(flexible footwear, participants' own footwear, and prototype footwear) were evaluated using repeated measures analysis of variance (ANOVA) with Bonferroni-adjusted post-hoc tests for pairwise comparisons. The effect sizes for all significant main effects were calculated using the eta-squared statistic (η^2) and were interpreted using the following cut-offs: 0 – 0.06 (small), >0.06 – 0.14 (medium) and >0.14 (large) [28]. Differences in perceptions of participants' own footwear versus the prototype footwear were evaluated using paired *t*-tests. Level of significance was set at 0.05.

Results

Participant characteristics

Participant characteristics are shown in Table 1, and characteristics of participants' own footwear are shown in Table 2. Two participants had missing data for the tandem walking test (due to an inability to complete the test) and were given the 'worst' score of the remaining sample.

Effects of footwear on balance

Results of the repeated measures ANOVAs for the balance tests are shown in Table 3. There was no overall

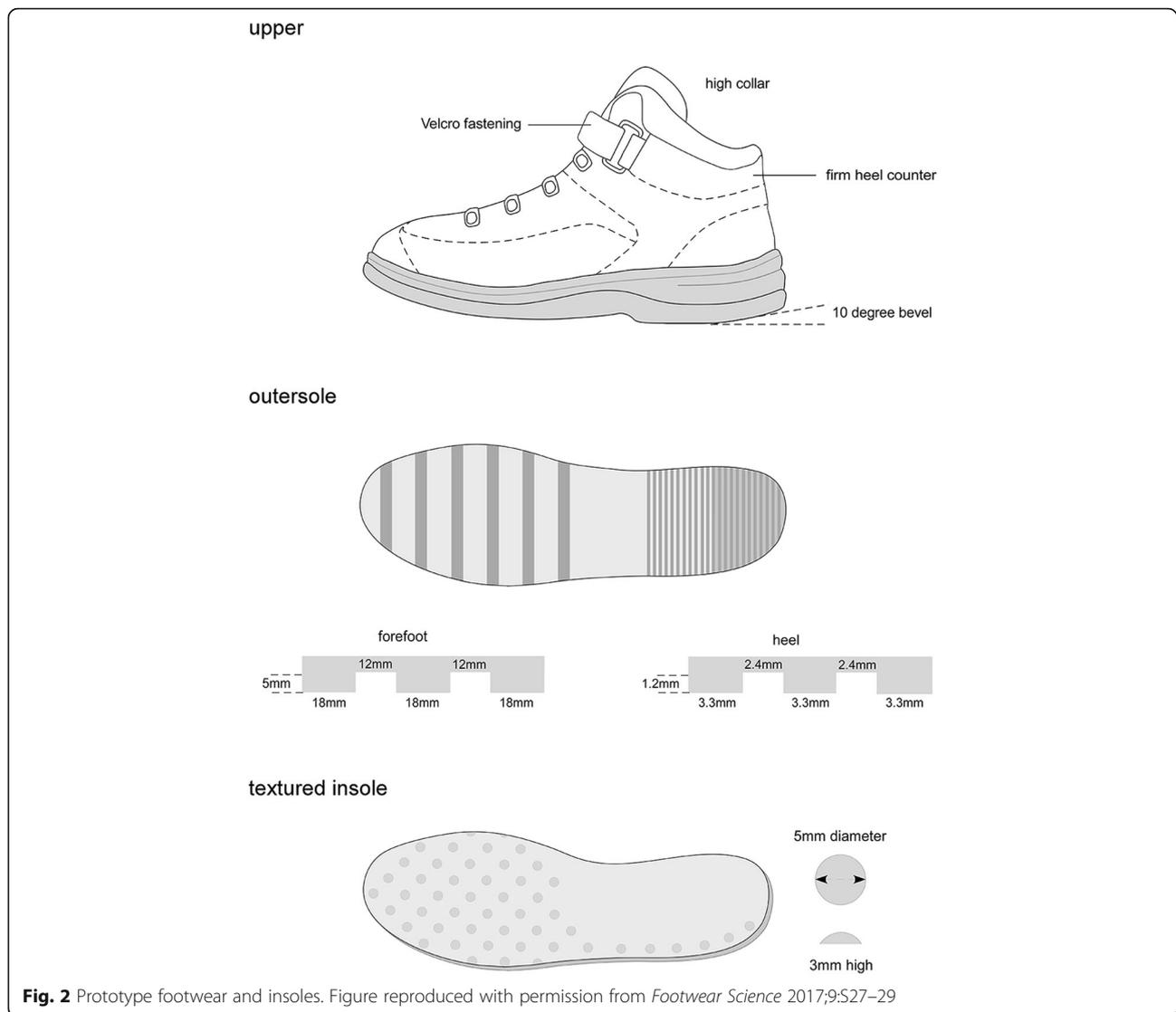


Fig. 2 Prototype footwear and insoles. Figure reproduced with permission from *Footwear Science* 2017;9:S27–29

effect of footwear on postural sway ($F = 2.6$, $P = 0.096$). For the limits of stability test, there was no overall effect of footwear on maximum excursion ($F = 0.5$, $P = 0.594$) or directional control ($F = 1.7$, $P = 0.206$). For the tandem walk test, there was no overall effect of footwear on speed ($F = 2.7$, $P = 0.086$). However, there was a significant overall effect of footwear on step width ($F = 9.3$, $P = 0.001$, $\eta^2 = 0.40$, large effect size), with post-hoc comparisons indicating that step width was significantly greater in the flexible footwear and own footwear compared to wearing the prototype footwear. There was also a significant overall effect of footwear on end sway ($F = 5.6$, $P = 0.009$; $\eta^2 = 0.29$, large effect size), with post-hoc comparisons indicating that end sway was significantly greater in the flexible footwear and own footwear compared to wearing the prototype footwear.

Effects of footwear on gait patterns

Results of the repeated measures ANOVAs for gait patterns are shown in Table 3. There was no significant overall effect of footwear on walking speed ($F = 1.7$, $P = 0.204$), cadence ($F = 1.9$, $P = 0.173$), step length ($F = 0.6$, $P = 0.544$) or step width ($F = 1.2$, $P = 0.303$).

Perceptions of footwear

Participants' perceptions of their own footwear and the prototype footwear are shown in Table 4. Participants perceived their own footwear to be more attractive, comfortable, well-fitted and easier to put on and off compared to the prototype footwear, but there was no difference in perceived heaviness. When asked if they would consider wearing the prototype footwear

Table 1 Participant characteristics

Age, mean (SD) years	74.4 (5.6)
Height, mean (SD) cm	158.9 (5.77)
Weight, mean (SD) kg	75.5 (12.8)
Body mass index, mean (SD) kg/m ²	29.9 (4.8)
Major medical conditions	
Heart disease	10 (33.3)
Diabetes	4 (13.3)
Stroke	3 (10.0)
Osteoarthritis	24 (80.0)
High blood pressure	18 (60.0)
Peripheral vascular disease	2 (6.7)
Short Form-12 Version 2	
Role – physical, mean (SD)	44.4 (9.5)
Role – mental, mean (SD)	54.2 (8.6)
Incidental and Planned Exercise Questionnaire total, mean (SD) hours/week	19.8 (14.8)
QuickScreen falls risk factors	
At least one falls risk factor	27 (90.0)
Fallen in past 12 months	7 (23.3)
Use of 4 or more medications	16 (53.3)
Use of psychotropic medications	16 (53.3)
Impaired visual acuity	15 (50.0)
Impaired peripheral sensation	6 (20.0)
Failed near tandem stance test	9 (30.0)
Failed alternate step test	12 (40.0)
Failed sit-to-stand test	10 (33.3)
Total falls risk score, mean (SD) ^a	3.3 (3.0)
Falls Efficacy Scale International, mean (SD) ^b	25.2 (7.4)
Foot problems	
Hallux valgus	14 (46.7)
Lesser toe deformity	20 (66.7)
Plantar keratotic lesions	20 (66.7)
Keratotic lesions on toes	12 (40.0)
Manchester Foot Pain and Disability Index	
Pain subscale, mean (SD) ^c	2.8 (2.6)
Functional limitation subscale, mean (SD) ^d	4.7 (4.0)

Values are *n* (%) unless otherwise stated

^ascore ranges from 1 to 8.6; higher score indicates greater risk

^bscore ranges from 16 to 64; higher score indicates greater fear (low 16–19, moderate 20–27, high 28–64)

^cRasch-transformed score ranges from 0 to 10; higher score indicates greater impairment

^dRasch-transformed score ranges from 0 to 20; higher score indicates greater impairment

to reduce their risk of falling, 18 (60%) said yes, 3 (10%) said no, and 9 (30%) said maybe. Of those who said no or maybe, appearance was the most commonly reported concern (*n* = 6, 50%).

Table 2 Characteristics of participants' own outdoor footwear

Shoe style	
Athletic shoe	8 (26.7)
Walking shoe	6 (20.0)
Sandal	5 (16.7)
Moccasin	4 (13.3)
Boot	4 (13.3)
Mary-Jane	2 (6.7)
High heel	1 (3.3)
Sole flexion point	
At MTPJs	18 (60)
Proximal to MTPJs	7 (23.3)
Distal to MTPJs	5 (16.7)
Heel height, mm – mean (SD), range	26 (9), 10–44
Sole thickness, mm – mean (SD), range	13 (6), 3–23
Sole hardness, Shore A – mean (SD), range	60 (19), 30–96
Weight, gm – mean (SD), range	265 (65), 130–359

Values are *n* (%) unless otherwise stated

Discussion

The primary objective of this study was to evaluate balance and gait patterns in older women while wearing three types of outdoor footwear: (i) flexible 'control' footwear, (ii) their own footwear, and (iii) prototype footwear and insoles designed to improve balance. Our findings indicate that performances on tests of postural sway and limits of stability did not differ between the three footwear conditions, nor were there any differences in temporospatial gait parameters (walking speed, cadence, step length or step width). However, balance performance when undertaking the tandem walking test was enhanced while wearing the prototype footwear, as evidenced by reductions in step width and postural sway at the completion of the test. These findings suggest that the prototype footwear may improve lateral stability in older women.

There are two main explanations for the lack of differences in postural sway, limits of stability and gait patterns between the footwear conditions. Firstly, the flexible footwear we used as the control condition had no features considered to be beneficial to balance, but equally had no features that were clearly hazardous. Participants' own footwear was also generally good, with many wearing athletic or walking footwear, which has been shown to be associated with the lowest falls risk [29]. A likely explanation for this is that most of the participants were recruited from a podiatry clinic database, where appropriate footwear would have been frequently emphasised. Secondly, these tests may not have been challenging enough to the postural control system, as the standing tests were conducted in a bipedal stance position and the walking tests were conducted on a level

Table 3 Differences in balance and gait patterns between the footwear conditions

	Flexible footwear	Own footwear	Prototype footwear	P value ^e
Balance				
Postural sway velocity, °/sec ^c	0.53 (0.19)	0.60 (0.26)	0.57 (0.21)	0.096
Limits of stability test				
Maximum excursion (% LOS) ^b	70.3 (15.6)	69.9 (17.4)	71.5 (15.7)	0.594
Directional control (%) ^d	57.4 (15.5)	54.0 (17.2)	55.1 (15.3)	0.206
Tandem walk test				
Speed, cm/sec ^d	17.8 (8.7)	19.4 (10.0)	18.3 (10.6)	0.086
Step width, cm ^c	11.6 (5.7)	10.2 (6.2)	7.4 (3.1) ^{ab}	0.001
End sway, °/sec ^c	5.9 (3.4)	4.9 (2.0)	4.1 (2.0) ^{ab}	0.009
Gait patterns				
Walking speed, cm/sec ^d	107.4 (18.1)	109.5 (19.2)	108.0 (17.8)	0.204
Cadence, steps/min ^c	110.8 (10.1)	112.0 (11.2)	111.1 (10.2)	0.173
Step length, cm ^d	58.0 (7.1)	58.5 (7.2)	58.2 (6.8)	0.544
Step width, cm ^c	59.1 (6.6)	59.6 (7.0)	59.4 (6.6)	0.303

Values are mean (SD)

^asignificantly different to flexible shoe

^bsignificantly different to own shoes

LOS limits of stability

^clower scores represent better performance

^dhigher scores represent better performance

^eP value for main effect of one-way ANOVA

surface. It is possible that greater differentiation between the footwear conditions may have been obtained by testing responses to postural perturbations [30] or by conducting the walking tests on an irregular surface [31].

The observed improvement in the tandem walk test when wearing the prototype footwear, however, is a notable finding, as several studies have demonstrated the importance of lateral stability in relation to risk of falling. Older people who fall have been shown to exhibit increased lateral sway when standing in bipedal [32, 33], near-tandem [34] and unipedal [35] positions, increased lateral stepping reactions to recover balance in response to postural perturbation [36, 37], and an increased stride width when walking [38]. We found that step width when undertaking the tandem walk test was significantly

narrower with the prototype footwear, which indicates that participants had less of a need for more lateral foot placement to control the lateral displacement of the centre of mass. Furthermore, postural sway was significantly reduced at the completion of the task, indicating better balance recovery in response to the lateral instability induced by tandem walking. Several features of the prototype footwear may have been responsible for this improvement, including the supportive heel collar (by providing mechanical resistance to excessive ankle movement [39] and enhanced tactile feedback of ankle position [40]), the large surface area of the sole [41, 42], and the textured insole providing tactile feedback relating to lateral displacement of the centre of mass [26, 27].

The secondary objective of this study was to investigate older womens' perceptions of the prototype footwear, as in order to be considered a practical intervention, such footwear needs to be acceptable to older people from the perspective of comfort, ease of use and aesthetics. Perhaps not surprisingly, participants perceived their own footwear to be more attractive, comfortable, well-fitted and easier to put on and off compared to the prototype footwear. However, when asked if they would consider wearing the prototype footwear to reduce their risk of falling, 60% said yes, 10% said no, and 30% said maybe, with the appearance of the footwear being the most commonly reported concern. This finding is encouraging, as the initial prototype was designed primarily with function in mind, and little attention was given to aesthetics. For example, the

Table 4 Differences in perceptions of own footwear and prototype footwear

	Own footwear	Prototype footwear
Attractiveness to self	62.9 (22.4)	44.0 (24.8)*
Attractiveness to others	57.1 (21.3)	37.1 (22.0)*
Comfort	84.2 (10.5)	64.0 (17.4)*
Fit	87.3 (7.0)	74.6 (14.9)*
Ease of donning and doffing	84.4 (14.7)	62.5 (20.9)*
Heaviness	30.1 (23.9)	39.5 (21.8)

Values are mean (SD) mm from 100 mm visual analog scales. Higher scores represent greater perceived attractiveness, comfort, fit, ease of donning and doffing and heaviness

*significant difference at $P < 0.01$

prototype footwear had a black leather upper and hiking boot-style eyelets; both features that could easily be modified to improve aesthetics without impacting greatly on function.

The findings of this study need to be interpreted in the context of methodological limitations. First, participants were only provided with a brief period of time to acclimatise to the different footwear conditions before undertaking the balance tests. This is likely to have disadvantaged the prototype footwear, as the leather upper was relatively stiff, and the high collar and textured insole would have been novel to most participants. Second, because women are more likely to fall and wear potentially hazardous footwear, we specifically recruited older women into the study, so we cannot be certain that the findings are generalisable to older men. Third, it could be argued that a frailer group of older women with a higher risk of falling may have been a more appropriate target sample. However, our prototype footwear is designed to be worn outdoors, and it has been shown that older people who fall outdoors are more physically active and healthy than those who fall indoors [43]. Fourth, our assessment protocol did not include any tests specifically targeting slip resistance, so the slip resistant features of the outsole of the prototype footwear were not directly evaluated. However, the outsole design features have previously been shown to enhance slip resistance in both mechanical tests [21, 22, 24, 25] and gait studies [23]. Finally, the protocol we used does not allow us to delineate the relative contribution of the footwear and insoles to balance performance.

Conclusion

This preliminary study has shown that the prototype footwear and insoles do not influence standing balance, leaning balance or temporo-spatial gait parameters, but improve balance when performing a tandem walk test, as evidenced by a narrower step width and decreased sway at the completion of the task. However, further research is required to evaluate the footwear under more challenging conditions (including responses to postural perturbation, and walking on irregular or slippery surfaces), and to modify the design to make the footwear acceptable to older women from the perspective of aesthetics and comfort. Finally, to determine whether wearing such footwear can contribute to the prevention of falls, a randomised trial using prospectively-documented incident falls as the primary outcome measure would need to be conducted.

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Availability of data and materials

The datasets used and/or analysed during the current study are available from the corresponding author on reasonable request.

Authors contributions

HBM was involved in all aspects of this study including study conception and design, obtaining funding, data collection, data analysis and interpretation, and drafting and critically revising the manuscript. MA was involved in study design, data collection, and critically revising the manuscript. SEM was involved in study conception and design, obtaining funding, data collection, data interpretation and critically revising the manuscript. All authors have read and approved the final manuscript.

Ethics approval and consent to participate

Ethical approval was granted from the La Trobe University Faculty of Health Sciences Human Ethics Committee (Reference FHEC14/254), and written informed consent was obtained from all participants prior to the study.

Consent for publication

Not applicable.

Competing interests

The prototype footwear tested in this study was manufactured by a footwear company (Dr Comfort®, Mequon, WI, USA) with a view to making the shoes commercially available if they are effective, and the company believes there is a sufficient market for them. No commercial arrangements or royalty agreements have been made, as this is an early proof-of-principle study. However, there is a possibility that the researchers, in their capacity as staff members of La Trobe University, may obtain some commercial benefit if the footwear reaches the market in the future. The authors have not received any reimbursements and do not hold any stocks or shares in the company, and are not currently applying for any patents related to the content of the manuscript. There are no non-financial competing interests.

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